# Full-thickness skin-on-a-chip model for *in vitro* drug testing



#### Patrícia Zoio, PhD Candidate Abel Oliva, Supervisor



### MOTIVATION



Increasing demand for the development of *in vitro* engineered skin models

Ethical regulations

-3R principles -Ban on animal testing (cosmetics) High prevalence of skin diseases

-Chronic (e.g., psoriasis, eczema) -Malignant (melanoma) Skin-targeted drug delivery

-Topical -Dermal -Transdermal

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Conventional in vitro skin model

#### 2D cell culture (keratinocytes and/or fibroblast)



- Complexity + reproducibility

Conventional 3D skin models (epidermal or full-thickness)



+ Complexity - reproducibility Weaker barrier than *in vivo* skin Lack mechanical stability

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Organ-on-a-chip technology

Combination of cell biology, engineering, biomaterial to simulate the microenvironment of the organ (tissue interfaces and mechanical stimulation)



+ Complexity + reproducibility







Protocol developed to generate a full-thickness skin model based on a fibroblast-derived matrix:



Dermis culture time



**Optimization of culture time:** 

- -Mature dermal equivalent
- -Epidermis support
- -Keratinocyte infiltration minimization

Increased expression of colagens and fibronectin with culture time



Dermal maturation affects epidermal development



Stratified squamous epithelium structured in basal, spinous, granular and corneal layers



Models were kept at ALI for up to 50 days and its structure monitored over time

#### Extended lifespan compared to conventional models

Reduction of epidermal thickness; Preserved architecture;

Models remain stable, maintaining the same thickness and epidermal layers;

A Macroscopic appearance



- FTSm with melanocytes
- FTSm w/o melanocytes

Development of a pigmented version of the FTSm with active melanocytes at the dermo-epidermal junction



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**METHODS ARTICLE** 

Pigmented Full-Thickness Human Skin Model Based on a Fibroblast-Derived Matrix for Long-Term Studies

Patrícia Zoio, MSc,<sup>1</sup> Sara Ventura, MSc,<sup>1</sup> Mafalda Leite, BSc,<sup>1</sup> and Abel Oliva, PhD<sup>1,2</sup>

FTSm with increased mechanical stability, excluding the use of animal-derived hydrogels;

Dermis formation in one week whereas other fibroblast-derived matrix approaches need 4 weeks;

FTSm with extended lifespan compared to conventional models;

Pigmented version of the FTSm with active melanocytes at the dermo-epidermal junction

accepted



## Open-source human skin model with an *in vivo*-like barrier for drug testing

Patrícia Zoio<sup>1</sup>, Sara Lopes-Ventura<sup>1</sup>, Joana Marto<sup>2</sup>, Abel Oliva<sup>1,3</sup>

In-depth analysis of the skin barrier function;

Drug testing performed according OECD TG;

Combining the FTSm based on a fibroblast-derived matrix with OoC technology



#### (b) Apical chamber (Polycarbonate) Apical Inlet Magnets Apical Outlet Scaffold (Polystyrene) Cell culture chamber (PDMS) PCR tape **Basal inlet Basal outlet** Basal chamber (Polycarbonate)

SoC designed to ensure **stability** during long-term culture while providing a **modular geometry** 

Double perfusion system: Continuous supply of nutrients and removal of metabolic waste products

Fabricated using CNC micromachining and laser cutting



#### PDMS cell culture layer



#### SoC devices placed in dedicated support



Protocol developed to generate a skin-on-a-chip model:



**Epidermis** 



Dynamic perfusion was achieved by connecting the inlet ports to a multichannel peristaltic pump. Flow rate 1.5 ul/min – 2 ul/min

Dynamic flow stimulates the production of endogenous FDM. Compared to the static culture, the dermis produced using dynamic flow resulted in increased deposition of ECM



Dynamic flow stimulates the production of endogenous FDM. Compared to the static culture, the dermis produced using dynamic flow resulted in increased deposition of ECM



Full-thickness models cultured for 20 days



Static

Static



Epidermal thickness 70±30 µm

Epidermal thickness 41±15 µm Both models show a stratified and differentiated epidermis after 11 days at ALI. No significant differences were detected concerning the thickness of the corneal layers

From the histological analysis, the major difference was the increased thickness of the epidermal compartment



SoC shows increased filaggrin expression, a skin barrier protein and differentiation marker, and increased involucrin expression. This points to an enhanced barrier function





Sensors were integrated into the OoC device for real-time TEER measurement during tissue formation

TEER measurements as a nondestructive technique to quantify the skin barrier. TEER reflects skin barrier functionality by measuring the overall barrier to ions.

TEER analysis used to evaluate the stage of skin differentiation





During culture for 2 weeks at ALI, there is an increase in TEER values, reflecting progressive SC accumulation and TJ formation; Values consistent with barrier function integrity

**Skin toxicity testing:** TEER measurements were performed while exposing the skin to a benchmark irritant for 3 h.





The impact of the irritant was also shown by the penetration of the LY

Drug testing can directly be performed on the platform, with key diagnostic parameters being monitored in real-time.

<b>*</b> **	micro
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Article Biomimetic Full-Thickness Skin-on-a-Chip Based on a Fibroblast-Derived Matrix

Patrícia Zoio <sup>1</sup>, Sara Lopes-Ventura <sup>1</sup> and Abel Oliva <sup>1,2,\*</sup>

Platform with a modular architecture that allows the leakage-free integration of a porous scaffold;

Dynamic flow applied during dermis generation increased ECM deposition;

Well-differentiated and organized epidermis with increased thickness and enhanced barrier function;

Permeation assays performed in situ;

**micromachines** 

#### Article

Barrier-on-a-Chip with a Modular Architecture and Integrated Sensors for Real-Time Measurement of Biological Barrier Function

MDP

Patrícia Zoio<sup>1</sup>, Sara Lopes-Ventura<sup>1</sup> and Abel Oliva<sup>1,2,\*</sup>

#### ➡

The integrated tetrapolar electrode configuration resulted in a more homogenous sensitivity distribution along the culture area

Integrated electrodes for real-time, non-destructive TEER measurements to monitor the tissue development;

Skin toxicity assays performed in situ;



### CONCLUSIONS



## ACKNOWLEDGMENTS

# THANK YOU

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# **THANK YOU**



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